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### Research Article

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# Sodium Chloride and Water Transport in the Descending Limb of Henle

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ABSTRACT The unique membrane characteristics of the thin descending limb of Henle (DLH) play an integral part in the operation of the countercurrent system. We examined these properties in vitro by perfusing isolated thin descending limbs of rabbits. Active transport of NaCl was ruled out by failure to demonstrate either net transport or transmembrane potential difference when perfusing with isosmolal ultrafiltrate of the same rabbit serum as the bath. Transmembrane potential was zero, and net fluid transport was  $-0.07 \pm 0.06$ nl mm<sup>-1</sup> min<sup>-1</sup>, which also is not significantly different from zero. Passive permeability coefficient for  $Na(P_{N*})$ was determined from the disappearance rate of <sup>22</sup>Na from isosmolal perfusion solution. P<sub>Na</sub> was surprisingly low, 1.61  $\pm 0.27 \times 10^{-5}$  cm sec<sup>-1</sup>, a figure which is significantly less than P<sub>Na</sub> in the proximal convoluted tubule (PCT). Reflection coefficient for NaCl ( $\sigma$ NaCl) was measured by perfusing the tubule with Na-free raffinose solution in a bath of rabbit serum to which sufficient NaCl was added to obtain conditions of zero net fluid movement. The measured  $\sigma$ NaCl of 0.96 ±0.01 is significantly greater than on NaCl in the PCT. Water permeability to osmotic gradients (L<sub>P</sub>) was determined by perfusing with ultrafiltrate of rabbit serum in a bath made hyperosmotic by addition of either 100 mOsm raffinose or NaCl.  $L_P$  with raffinose was 1.71  $\pm 0.15$  $\times$  10<sup>-4</sup> ml cm<sup>-2</sup> sec<sup>-1</sup> atm<sup>-1</sup> and with NaCl 1.62  $\pm 0.05 \times$ 10<sup>-4</sup> ml cm<sup>-3</sup> sec<sup>-1</sup> atm<sup>-1</sup>, indicating much greater water permeability than in the PCT. In each case the measured increase in osmolality of the collected fluid was primarily due to water efflux without significant influx of solute.

The finding of low permeability to sodium and high

permeability to water is consonant with the hypotheses that high interstitial concentration of Na in the medulla generates an effective osmotic pressure which results in concentration of the fluid as it courses through the DLH primarily by abstraction of water without significant net entry of NaCl.

#### INTRODUCTION

The tubular fluid in the descending limb of Henle (DLH) becomes progressively more concentrated as it travels from the corticomedullary junction towards the papillary tip. The mechanism by which this takes place is not clear. Two basically different ways may be postulated. First, water may be primarily abstracted without influx of solute. Alternatively, influx of solute may predominate with only minimal efflux of fluid. These two mechanisms demand entirely different membrane characteristics. In the former hypothesis the membrane would be quite permeable to water but relatively impermeable to NaCl, while in the latter hypothesis the membrane would require a high permeability to NaCl.

The relative inaccessibility of the thin, descending loop of Henle to conventional micropuncture techniques has prevented previous quantitative evaluation of its passive permeability properties. The present study was designed to obtain this information by in vitro perfusion of isolated segments of DLH dissected from rabbit kidneys. The results of direct measurements of the hydraulic permeability to water (L<sub>P</sub>), passive permeability to NaCl (P<sub>Na</sub>), and reflection coefficient of NaCl ( $\sigma$ NaCl) will be presented together with measurements of those membrane characteristics which allow for evaluation of active tranpsort of NaCl. The combination of these properties will be discussed with reference to the mechanism by which the intraluminal fluid of the DLH becomes hyperosmotic.

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FIGURE 1 Diagrammatic illustration of the method by which thin descending limbs of Henle are perfused in vitro. The holding pipette at the perfusion end has an I.D. of  $36-40 \mu$ . The perfusion pipette 0.D. ranges from 12 to  $20 \mu$ . The collecting pipette I.D. is  $22-24 \mu$ . Fluid is periodically sampled from the collecting pipette with a constant bore calibrated pipette. The bathing chamber holds 1.25 cc of fluid.

#### METHODS

Isolated segments of thin descending limbs of Henle were perfused by the general techniques described (1) for the PCT of rabbit. Schematic representation of these experiments is given in Fig. 1, and actual photographs of perfused loop are shown in Figs. 2 and 3. Female New Zealand white rabbits weighing 1.5-2.5 kg were used in all experiments. After the rabbit was decapitated by use of a guillotine, the kidney was quickly removed, and cut horizontally in 1- to 2-mm slices, and segments of these slices were transferred into chilled dishes of rabbit serum where the individual loop was dissected free without use of collagenase or other enzymatic agents. Positive identification was obtained by dissecting the loop intact with the pars recta. Most of the nephrons perfused were from the mid-medullary region. After dissection the distal end of the loop was cut with microscissors, followed by removal of the pars recta in a similar manner. The remaining descending thin limb was transferred into a perfusion dish of rabbit serum which was kept at 37°C and pH of 7.4 by continuous bubbling with 5% CO<sub>2</sub>-95% O<sub>2</sub>. The tubule was then picked up by suction into small pipettes and perfused by means of a concentric glass pipette, as illustrated in Fig. 1. Good electrical seal was obtained at the collecting end by placing a small quantity of Sylgard-184 (Dow Corning Corp., Midland, Mich.) at the tissue-glass junction in the collecting pipette (2). Colored mineral oil was placed on top of the collected fluid to minimize evaporation. During each experiment three control periods were obtained at 10-min intervals. After this the desired experimental manipulation was performed, and three additional 10-min collections were obtained. In this manner, each individual tubule acted as its own control.

Active transport of NaCl by the thin descending limb was evaluated by measuring (a) transmembrane potential and (b) the magnitude of net fluid transport. The transmembrane potential was measured by placing a Ag-AgCl electrode into the perfusion pipette containing isomolal ultrafiltrate of the same rabbit serum as that used in the bath. A similar reference electrode was connected to the bath by an agar bridge. The circuit was completed by placing a voltage reference source and a General Radio Company (West Concord, Mass.) Model 1230-A electrometer in the circuit by techniques similar to schematics previously published (3). Any observed voltage was adjusted to zero before perfusion of the individual tubule, and this adjustment was checked at the end of the experiment. Two experiments were discarded because of a greater than 3 mv drift in the base line during the course of the experiment. Perfusion pipettes with relatively large bores  $(I.D. = 20 \mu)$  were advanced at least  $500 \mu$  down the lumen of the tubule to give adequate electrical seal at the perfusion end. The tip resistances ranged from 4 to 7 m  $\Omega$ . In these experiments the rate of perfusion was governed by hydrostatic pressure of the perfusion fluid and was varied from 30 nl min<sup>-1</sup> to such a low flow rate that the tubule tended to collapse around the inner perfusion pipette.

Net fluid transport was measured at slow perfusion rates, 6.21  $\pm 0.35$  nl min<sup>-1</sup>, using the same bath and perfusion solution as that in the transmembrane potential measurements. Albumin-<sup>125</sup>I was added to the perfusion solution to give final counts ranging from 40 to 80 cpm/nl. Perfusion rate (V<sub>1</sub>), collection rate (V<sub>0</sub>), and absolute reabsorption were calculated from concentration changes in collected <sup>125</sup>I by equations previously published by Burg and Orloff (4):

$$C = \frac{V_i - V_o}{L}$$
(1)

where  $V_1$  is calculated by dividing the <sup>125</sup>I cpm of the collected fluid by <sup>125</sup>I cpm/nl of perfusion fluid and by time of the collection period.  $V_{\circ}$  is obtained directly by a calibrated constant bore collection pipette. L is the length of the tubule, and C is the absolute volume of fluid transported in nl mm<sup>-1</sup>min<sup>-1</sup> and is positive if fluid is absorbed and negative if fluid is secreted.

The total radioactivity secondary to albumin-<sup>125</sup>I in each collected sample varied from 4000 to 15,000 counts per 10 min. The samples routinely were preset for 10-min counts. If 10% of the label were lost into the bath during the 10-min collection period, then the total bath counts would vary from 400 to 1500 counts per 10 min. However, when the total bath was counted, there were no detectable counts. It is therefore felt that albumin-<sup>125</sup>I is a suitable volume marker. Tissue uptake of albumin-<sup>126</sup>I could be only a trivial source of error, since each tubule is perfused for 20 min before the first collection. Thus, there is more than adequate time for equilibration of albumin-<sup>126</sup>I in a tissue with less than 1 nl total volume.

Passive permeability coefficient for <sup>22</sup>Na (P<sub>Ns</sub>) was estimated from the disappearance rate of <sup>22</sup>Na from the perfusion fluid. The perfusion fluid, which was isomolal ultrafiltrate of the same rabbit serum as used in the bath, was perfused at a mean rate of 19.6  $\pm$ 0.4 nl min<sup>-1</sup>. The passive

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permeability coefficient of Na was estimated according to the following expression (5):

$$P_{Na} = \frac{V_i}{A} \ln \frac{C_i^*}{C_o^*}$$
(2)

where A = area of tubule,  $V_1$  = perfusion rate,  $C_1^* = cpm/nl$  of <sup>22</sup>Na in perfusion fluid, and  $C_0^* = cpm/nl$  of <sup>22</sup>Na in the collected fluid. This equation is applicable when  $J_v = 0$  and gives the passive permeability of <sup>22</sup>Na in both directions in absence of active transport.

The reflection coefficient,  $\sigma$ , as defined by Staverman (6), is equal to

$$\sigma = \pi \text{ observed}/\pi \text{ theoretical}$$
(3)

where  $\pi$  equals the osmotic pressure secondary to solute in question. This operational definition indicates the effectiveness of a solute in generating an osmotic pressure across a membrane as compared with an equivalent concentration of an ideal nonpenetrating molecule. Kedem and Leaf (7) have shown that this definition of  $\sigma$  is applicable for either nonelectrolytes or electrolytes, provided the electrolyte is treated as a single electronically neutral component; under these conditions the electrical field across the membrane may be neglected. A completely permeant compound cannot exert any osmotic force and would have  $\sigma = 0$ , while a completely impermeant compound would exert its theoretical osmotic pressure and have  $\sigma = 1$ . In these experiments the reflection coefficient of raffinose is assumed to equal 1.0, since Marsh and Solomon (8) have shown by the split-drop technique that raffinose is completely impermeant in the DLH. Further justification for this assumption comes from our experiments where it was noted that over 99% of perfused mannitol-<sup>14</sup>C could be accounted for in the collected fluid when it was added to the perfusion fluid of isosmolal ultrafiltrate. Unfortunately, labeled raffinose is not available, but it is reasonable to expect that raffinose with a molecular weight of 594 is less permeant than mannitol with a molecular weight of 182.

 $\sigma$ NaCl was determined from experiments in which the perfusion solution was sodium-free and contained 293 mOsm of raffinose, 5 mM KCl, 1 mM MgCl<sub>2</sub>, and 1 mM CaCl<sub>2</sub>. Control periods were obtained by perfusing with isosmolal raffinose solution against a bath of rabbit serum. Average perfusion rate was 18.0 nl min<sup>-1</sup>. Tubule lengths ranged from 0.90 to 1.36 mm, with a mean length of 1.20 mm. During these periods there was a net influx of water owing



FIGURE 2 Photograph of the perfusion and collection end of a thin descending limb of Henle  $(\times 100)$ . A shows how the tubule appears at the perfusion end. Note that all of the pars recta is sucked into the constriction of the holding pipette, providing a good tissue-glass seal. B demonstrates the manner in which Sylgard-184 lightly constricts the tubule to provide excellent electrical seal.



FIGURE 3 Magnification  $(\times 400)$  of a perfused descending limb of Henle. From this it is evident that the outside and inside diameters are approximately the same. Only the nucleus of the squamous epithelium protrudes into the lumen. The cytoplasm appears quite clear, without granular material at the magnification.

to the higher effective osmolality of the perfusion solution. NaCl was then added to the bath for a final osmolality of 407. This reversed the net transport of fluid. Conditions of zero flow were obtained by interpolation between the control and hyperosmotic points. The  $\sigma$ NaCl at  $J_{\tau} = 0$  is  $\Delta \pi$  raffinose/ $\Delta \pi$  NaCl, where  $\Delta \pi$  raffinose is equal to the osmotic pressure of the luminal fluid.  $\Delta \pi$  NaCl is the osmotic pressure of the bath corrected for the mean osmotic pressure secondary to NaCl in the intraluminal fluid. The mean intraluminal NaCl concentration was assumed to be one-half the measured chemical NaCl was then approximated by multiplying the mean intraluminal concentration by the osmotic coefficients for NaCl.

Hydraulic conductivity of water  $(L_p)$  was determined by measuring net fluid movement in response to imposed osmotic gradients. During the control period the perfusion fluid was isosmolal ultrafiltrate of the same rabbit serum as that in the bath. Net fluid movement was then induced by addition of either 100 mOsm of raffinose or NaCl to the bath. Rapid perfusion rates and short segments, average length 472  $\mu$ , of tubules were chosen so that osmotic equilibration was not complete. Osmolality of the collected fluid was measured, and the logarithmic mean osmotic gradient between the bath and the collected fluid was obtained by use of semi-log paper.  $L_p$  was calculated in each case by the following equation:

$$L_{p} = \frac{J_{v}}{\pi B/P}$$
(4)

where  $\pi B/P$  is the logarithmic mean of the osmotic pressure difference between the bath and perfusion fluid. J<sub>v</sub> is the net induced water flow between the control and hyper-osmotic periods.

Human albumin-<sup>125</sup>I, which was routinely used as the volume marker, was purchased from E. R. Squibb & Sons (New York) and concentrated to contain approximately  $300 \ \mu Ci/cm^3$  by the use of Aminco (American Instrument

Co., Inc., Silver Spring, Md.) pressure dialysis using PM-10 filters. Before use it was dialyzed in a cellophane bag against a Ringer's solution to minimize the free <sup>125</sup>I. <sup>22</sup>Na was obtained from International Chemical & Nuclear Corporation, Burbank, Calif.). All isotopic counting was done on a Packard Model 3003 three-channel autogamma spectrometer (Packard Instrument Co., Inc., Downers Grove, Ill.). The ultrafiltrate of rabbit serum was made by pressure dialysis using Aminco PM-50 membranes. The osmolality of the collected fluid was determined by a Clifton nanoliter osmometer (Clifton Technical Physics, New York), in which the sample plate had been modified to obtain more reproducible measurements. The chemical Na of the collected fluid was determined by Aminco Helium glow photometer. All results are expressed as mean ±standard error.

#### RESULTS

Active transport was evaluated by perfusing tubule segments ranging in length from 1.05 to 2.80 mm at rates of 6.21  $\pm$ 0.35 nl min<sup>-1</sup> using isosmolal ultrafiltrate of the same rabbit serum as the bath. (The mean luminal diameter was 27  $\pm$ 0.07  $\mu$ .) Net transport in six consecutive experiments (18 collections) was  $-0.07 \pm 0.06$ nl mm<sup>-1</sup> min<sup>-1</sup>, which is not significantly different from zero (Table I). The collected fluid Na concentration was 142.8  $\pm$ 3.2 mEq/liter as compared with a bath Na concentration of 144.9 mEq/liter.

Transmembrane potential was  $-0.83 \pm 0.28$  mv (n = 6; lumen negative) using the same perfusion solution and bath as was used to evaluate net transport (Table I).

Passive permeability. Sodium permeability was measured isotopically using isosmolal ultrafiltrate as the perfusion fluid. The bath was rabbit serum. Net fluid

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 TABLE I

 Membrane Characteristics of the Thin Descending

 Limb of Henle

Net transport of fluid (C)	$-0.07 \pm 0.06$ nl mm <sup>-1</sup> min <sup>-1</sup>
Transmembrane potential (PD)	$-0.83 \pm 0.28 \text{ mv}$
Passive permeability coefficient	
for NaCl (P <sub>Na</sub> )	$1.61 \pm 0.27 \times 10^{-5} \text{ cm sec}^{-1}$
Hydraulic conductivity (Lp)	$1.71 \pm 0.15 \times 10^{-4}$
	ml cm <sup>-2</sup> sec <sup>-1</sup> atm <sup>-1</sup>
Reflection coefficient for NaCl	
(oNaCl)	$0.96 \pm 0.01$

movement was zero, while the mean perfusion rate was 19.6  $\pm 0.4$  nl min<sup>-1</sup> (n = 6). The short contact times and impermeability of the membrane allowed only 6.4% of the intraluminal sodium to exchange with the bath; however, significant differences were obtained in cpm of <sup>22</sup>Na between perfusion and collected fluids. Under these conditions P<sub>Na</sub> was 1.61  $\pm 0.27 \times 10^{-8}$  cm sec<sup>-1</sup> (n = 6) (Table I).

Reflection coefficients. The reflection coefficient for NaCl was measured by determining that concentration of NaCl in the bath at which the net transport of fluid was zero when perfusing with 309 mOsm of Na-free raffinose solution. In these experiments there was a net entry of NaCl ranging from 10.9 to 33.1 mEq/liter with a mean of 19.1 mEq/liter when the bath was



FIGURE 4 Measurement of reflection coefficient for NaCl in the thin descending limb of Henle. Net water flow,  $J_v$ , is represented on the coordinate. Negative values indicate influx of water into the lumen, while positive values represent abstraction of fluid from the nephron. The abscissa represents the osmolarity of the bath. Osmolarity of the perfusion fluid is 309. Each dot represents an average of three collection periods in an individual tubule. A line is drawn to connect the "control" and "experimental" points of the same tubule. Zero flow is obtained from the point at which the line intersects the horizontal axis. Corrected  $\sigma$ NaCl is calculated by methods described in the text.

309 mOsm of rabbit serum; when the bath concentration of NaCl was raised by 100 mOsm/liter, the Na concentration in the collected fluid ranged from 12.7 to 47.2 mEq/liter with a mean of 27.3 mEq/liter. Onehalf of the collected NaCl concentration was subtracted from bath NaCl to give  $\Delta \pi$  NaCl. At  $J_{\pi} = 0$ ,  $\sigma$ NaCl  $= \Delta \pi$  raffinose/ $\Delta \pi$  NaCl. The individual experimental results are depicted in Fig. 4.

The approximate 5% error in the estimation of  $\sigma$ NaCl arises from the correction factors used to calculate  $\sigma$ NaCl. Two assumptions account for the dual finding of some variability in the means and the very low standard error for each mean. First, the correction of the magnitude of NaCl gradient by estimation of the geometric mean intratubular concentration approximates, but cannot exactly equal, the NaCl gradient along the course of the measured length of DLH. Second, the assumption that the average raffinose concentration along the length of perfused tubule is the same as the perfusate is not exactly true in every instance. For example, when the bath is 309 mOsm/liter, there is net secretion of fluid and dilution of the raffinose, while with a hyperosmotic bath water is abstracted and the raffinose concentrated. The sources of error may be best exemplified by considering the raw data from a single experiment (Table II). If these values are substituted into the flow equation of Kedem and Katchalsky (9)  $J_{\tau} = -L_{P} (\pi \text{ raffinose} - \sigma \text{NaCl} \pi \text{ NaCl}), \text{ the } \sigma \text{NaCl may}$ be solved for directly since the other parameters are

 TABLE II

 Data from a Typical Single NaCl Reflection

 Coefficient Experiment

Length: 1.28 mm; inside diameter: 28  $\mu$ ; area: 11.3  $\times$  10<sup>-4</sup> cm<sup>2</sup>; area/mm: 8.84  $\times$  10<sup>-4</sup> cm<sup>2</sup>; perfusion fluid: 293 mOsm of raffinose; 5 mM KCl; 1 mM CaCl<sub>2</sub>; 1 mM MgCl<sub>2</sub>

Bath No. 1	Experimental data	Bath No. 2
15.9	$V_i$ (nl min <sup>-1</sup> )	17.7
-1.12	$J_{v}$ (nl mm <sup>-1</sup> min <sup>-1</sup> )	2.56
19.9	[Na] CF (mEq liter <sup>-1</sup> )	15.8
312	CF osmolality (mOsm)	403
275	mean $\Delta \pi$ NaCl (mOsm)	379
282	mean $\Delta \pi$ raffinose (mOsm)	313

The mean  $\Delta \pi$  raffinose of the intraluminal fluid is not the same as that of the collected fluid but may be represented as the logarithmic mean between the concentration of raffinose in the perfusion fluid and collection fluid. The mean  $\Delta \pi$  NaCl is obtained by subtracting one-half the NaCl osmolality in the collection fluid from the respective MaCl osmolalities of the two bathing media. CF = collected fluid. Bath No. 1 is rabbit serum, 309 mOsm. Bath No. 2 is 309 mOsm of rabbit serum plus 100 mOsm of NaCl for total osmolality of 409.

known. The independently determined  $L_P$  of  $1.71 \times 10^{-4}$ ml cm<sup>-2</sup> sec<sup>-1</sup> atm<sup>-1</sup> will be used in the solution of this equation. "NaCl equals 1.00, using the values from the experiments in which the bath was isosmolal, and 0.86, using the data from the experiments where hyperosmolal bath was used. The discrepancies in all probability arise from the correction factors used. As will be noted, the  $\sigma$ NaCl of 0.96 is in close agreement with 1.00 as calculated from the isosmolal conditions. This is to be expected since under these conditions the percentage transport of fluid is less than when hyperosmolar serum is used. Additional lines of evidence which heavily favor the higher oNaCl are obtained from the experiments, presented below, where the osmotically induced water flow is the same when equiosmolal quantities of NaCl or raffinose are used as the osmotic gradient. The two independent lines of evidence strongly support the validity of the high  $\sigma$ NaCl calculated by the simple assumptions presented, but the sources of error are recognized.

Osmotic water permeability. The hydraulic conductivity (L<sub>P</sub>) was calculated from experiments where net water movement was induced by addition of 100 mOsm/ liter of raffinose or NaCl to the bath. By perfusing short tubules,  $472 \pm 24 \mu$  in length, (n = 12) at a fast perfusion rate, 27.7  $\pm 1.3$  nl min<sup>-1</sup>, it was possible to collect perfusate before osmotic equilibration took place. In control periods the osmolality of the ultrafiltrate was 309, which was the same as the bath of rabbit serum. The osmolality of the bath was 407 in each case when raffinose or NaCl was added to the bath. The osmolality of the collected fluid then ranged from 355 to 396 with a mean osmolality of 379  $\pm 3.4$ . The mean L<sub>P</sub> was 1.71  $\pm 0.15 \times 10^{-4}$  ml cm<sup>-2</sup> sec<sup>-1</sup> atm<sup>-1</sup> (n = 6) (Table I) when the bath was made hyperosmolal by addition of

Mean  $\pm sE$ 

100 mOsm/liter of raffinose and  $1.62 \pm 0.05 \times 10^{-4}$  ml cm<sup>-2</sup> sec<sup>-1</sup> atm<sup>-1</sup> (n = 6) when 100 mOsm/liter of NaCl was added to the bath. In the experiments where the bath hyperosmolality was achieved by the addition of NaCl (Table III), the mean osmolality of the collection fluid increased by 69.7  $\pm 3.5$  mOsm or 22.5  $\pm 1.2\%$ . In these same experiments there was a net efflux of water which amounted to 22.3  $\pm 0.7\%$  of the perfusion rate.

The validity of the results thus far presented depends on the viability of the artificially perfused descending limb of Henle. Specifically, active transport of NaCl has been ruled out, and the absence of transmembrane potential leaves one wondering if the tissue is dead. It is impractical to measure oxygen consumption of a single perfused tubule since its total weight is less than 1 ng. To test the viability of DLH the effects of cyanide were tested. First, when 10<sup>-2</sup> м NaCN was added to the bath, the cells were noted to become granular and nuclei pyknotic. Second, when 0.25% Trypan blue is added to the bath, cells of the perfused DLH become stained in the presence of cyanide but not in its absence. Staining with Trypan blue is routinely used as an index of viability in lymphocyte experiments-viable cells not staining, while dead cells take up the dye. The third line of evidence to indicate that the isolated perfused DLH is alive arises from permeability studies. It is generally accepted that tissue becomes more permeable with death. It would be unusual to find the DLH as impermeable to <sup>22</sup>Na as reported here if it were not viable. Three separate experiments were conducted in which <sup>22</sup>Na permeability was measured in the presence and absence of 10<sup>-2</sup> M NaCN. After a 10 min exposure to NaCN, the tubule became markedly more permeable to <sup>22</sup>Na; and during the third collection period, Na

Exp. No.	Length	Area	$\mathbf{V}_{\mathbf{i}}$	J•	Collection fluid	% Increase in collection fluid	% Reabsorp. of fluid	$L_p$
	μ	$cm^2  imes 10^{-4}$	nl min <sup>-1</sup>	nl mm <sup>-1</sup> min <sup>-1</sup>	mOsm	mOsm		$ml \ cm^{-2} \ sec^{-1} \ alm^{-1} \\ \times \ 10^{-4}$
1	460	4.18	28.10	6.65	370	19.7	23.7	1.71
2	536	4.54	27.16	6.66	366	18.4	24.5	1.48
3	560	6.15	29.78	6.65	391	26.5	22.3	1.72
4	545	5.65	29.87	6.97	384	24.3	23.3	1.71
5	419	5.39	32.19	6.55	376	21.7	20.3	1.42
6	335	3.16	23.67	4.60	385	24.6	19.4	1.68

TABLE III

The Relationship between P	er Cent Increase in (	Osmolarity of the Collected	Fluid to Per Cent Reabsorption of	f
Fluid when the	he Bath is Made Hy	perosmolar by Addition of	100 mOsm of NaCl	

Control experiments were obtained using isosmolal ultrafiltrate of same rabbit serum as the bath.  $J_v$  is the difference in fluid reabsorption between control periods and when 100 mOsm of NaCl was added to the bath.  $V_i$  = perfusion rate (average of three collection periods),  $L_p$  = hydraulic conductivity of water.

 $22.5 \pm 1.2$ 

 $22.3 \pm 0.7$ 

 $1.62 \pm 0.05$ 

permeability had increased by over an order of magnitude. It is difficult to quantitate the increase in Na permeability to any greater degree than the general comments made since a new steady level of permeability was never reached. In each collection period the tubule became more permeable than in the previous period. These three lines of evidence strongly support the thesis that the tubule is viable.

#### DISCUSSION

The present studies provide further information concerning the role of the descending limb of Henle in the countercurrent multiplication system. Several lines of evidence indicate that the DLH does not actively transport NaCl. First, it was shown that the tubule is unable to transport net amounts of fluid in the absence of osmotic gradients. This finding is in agreement with the earlier in vivo studies of Marsh and Solomon (8), where they were able to show by the split-drop technique that the thin descending limb is not able to transport net amounts of fluid. Also, Morgan and Berliner (10) have shown that TF/P inulin does not change when the descending limb is perfused with solutions isosmotic to the medullary interstitium. Active salt transport might not be apparent from these techniques if the descending limb were sufficiently impermeable to water to prevent the reabsorption of the split drop or change in observed TF/P inulin. In the latter hypothesis if active salt transport were occurring in a relatively water-impermeable DLH, there should be a progressive decrease in NaCl concentration of the intraluminal fluid. In the present studies, the NaCl concentration in the collected fluid did not differ significantly from the bath NaCl, indicating that the thin limb of Henle cannot generate NaCl concentration gradients as has been hypothesized for the ascending thin limb. In the case of frog skin it is difficult to show net transport of fluid; however, the skin is able to transport Na actively as shown by the existence of transmembrane potential and short-circuit current (11). We therefore measured the transmembrane potential of the DLH and found it not to differ significantly from zero. On the basis of these results it appears that the isolated DLH does not actively transport salt; and hence, if it has the same properties in vivo as in vitro, then the DLH does not appear to play a role in generating medullary hypertonicity, but rather, it functions primarily as a passive equilibrating segment.

Numerous investigators (12–15) have found that the osmolality of the intratubular fluids becomes progessively hyperosmotic from the corticomedullary junction to the papilla. Disagreement, however, has arisen as to whether this occurs primarily by abstraction of fluid or by influx of solute. Lassiter, Gottschalk, and

Mylle (16) and Gottschalk et al. (12) have found that the DLH fluid to plasma inulin concentrations of TF/P inulin was approximately 11, which was much higher than in the last accessible part of the proximal convoluted tubule (PCT). This would suggest that fluid in the DLH becomes hypertonic primarily by abstraction of water. Recently de Rouffignac and Morel (17) have presented conflicting results and have suggested that 85% of the concentration in the DLH occurs by influx of solute, primarily NaCl.

Quantitation of volume reabsorption in the DLH from measured TF/P inulin values is hazardous since the TF/P inulin at the end of the pars recta cannot be determined by conventional micropuncture techniques. Recently, Marsh (18) has overcome this objection by puncturing the DLH at different levels. He measured the TF/P inulin and TF/P osmolality at these two puncture sites and concluded that both of these values increased by the same fractional amount in the more distal site. Though his (18) changes in TF/P values were small, they suggest that fluid abstraction is more significant than solute influx.

To completely evaluate the process of osmotic equilibration in the DLH it is necessary to determine the relative permeabilities to NaCl and water. No direct measurements of isotopic permeability to NaCl have been made, though indirect studies of de Rouffignac and Morel (19) would suggest high Na permeability in the DLH. They concluded from previous studies, in which <sup>22</sup>Na was injected into PCT and its disappearance rate was monitored in the urine, that the walls of the thin limb of Henle are quite permeable to sodium. This type of study makes the assumption that the pars recta is relatively impermeable to NaCl, which is in contrast to current thinking.

Direct measurements of PNa of the DLH in the present studies do not support the view of de Rouffignac and Morel. The P<sub>Na</sub> value of  $1.61 \times 10^{-5}$  cm sec<sup>-1</sup> is approximately 5-6 times less than the value in the proximal convoluted tubule.1 Further evidence that the DLH is relatively impermeable to NaCl is the high vaue for  $\sigma$ NaCl (0.96). This is in contrast to the much lower  $\sigma$ NaCl reported for the PCT (20-22). The high  $\sigma$ NaCl is consistent with the low isotopic permeability to NaCl and indicates NaCl is able to generate a high effective osmotic pressure. It also suggests that solvent drag of NaCl is minimal in this segment. It has been pointed out by Gottschalk and Mylle (15) that the  $L_P$  in DLH should be high since apparent osmotic equilibration between the vasa recta and luminal fluid takes place. The direct measurements presented here are consistent

<sup>&</sup>lt;sup>1</sup>Kokko, J. P., M. B. Burg, and J. Orloff. 1970. Characteristics of NaCl and water transport in the renal proximal tubule. Submitted for publication.

with the hypothesis put forth by Gottschalk and Mylle (15) and also are in agreement with the high water permeability demonstrated by Morgan and Berliner (10). The high  $L_P$  of 1.71  $\pm 0.15 \times 10^{-4}$  ml cm<sup>-2</sup> sec<sup>-1</sup> atm<sup>-1</sup> shows that the thin descending limb has much higher permeability to osmotic flow of water than previously had been found for the PCT (23).<sup>1</sup> Two qualifications must be made. These studies represent step functions, whereas the loop experiences osmotic gradients which are in linear differential increments. Under the current experimental conditions it was not practical to use shorter segments or smaller gradients. However, it is estimated that the net osmotic gradient of 100 mOsm induced for a mean length of 472  $\mu$  of DLH is approximately the same as seen by equivalent lengths of descending limb in vivo in a nondiuretic animal. The second qualification is that our studies were primarily performed at normal serum concentrations. It is possible that some of the coefficients measured in these studies may change in hyperosmotic surroundings; however, the hypothesized changes are not expected to be of major magnitude.

We next examined how the determined parameters, high  $L_{\rm P}$ , high  $\sigma$ NaCl, and low sodium permeability, are operative in concentrating the intraluminal fluid. These studies were performed by perfusing with 309 mOsm of ultrafiltrate against a bath made hyperosmotic by addition of 100 mOsm of NaCl. As summarized in Table III the omolality of the collected fluid increased by 22.5%, while the net efflux of water was equal to 22.3% of the perfusion rate. Thus, it can be seen that the concentration of the descending loop fluid occurs almost entirely by abstraction of water without significant net entry of NaCl.

In summary, these studies show that the isolated descending loop of Henle does not actively transport NaCl and therefore does not contribute to generation of medullary hypertonicity; instead, it appears to serve entirely as a passive equilibrating segment. The combination of high osmotic permeability to water and low permeability to Na is consistent with the hypothesis that high interstitial concentration of Na in the medulla generates an effective osmotic pressure which results in concentration of the fluid as it comes through the DLH primarily by abstraction of water without significant net entry of NaCl.

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